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TWO-HOP TELEMETRY INTERFACE FOR MEDICAL DEVICE

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TWO-HOP TELEMETRY INTERFACE FOR MEDICAL DEVICE

TECHNICAL FIELD

5 This document relates generally to medical systems, devices, and methods, and particularly, but not by way of limitation, to a two-hop telemetry interface for a medical device such as an implantable cardiac rhythm management device.

BACKGROUND

10 When functioning properly, the human heart maintains its own intrinsic rhythm. Its sinoatrial node generates intrinsic electrical cardiac signals that depolarize the atria, causing atrial heart contractions. Its atrioventricular node then passes the intrinsic cardiac signal to depolarize the ventricles, causing ventricular heart contractions. These intrinsic cardiac signals can be sensed on a surface electrocardiogram (ECG) obtained from electrodes placed on the patient's skin, or
15 from electrodes implanted within the patient's body. The surface ECG waveform, for example, includes artifacts associated with atrial depolarizations ("P-waves") and those associated with ventricular depolarizations ("QRS complexes").

A normal heart is capable of pumping adequate blood throughout the body's circulatory system. However, some people have irregular cardiac rhythms, referred
20 to as cardiac arrhythmias. Moreover, some patients have poorly spatially-coordinated heart contractions. In either case, diminished blood circulation may result. For such patients, a cardiac rhythm management system may be used to improve the rhythm and/or spatial coordination of heart contractions. Such systems are often implanted in the patient and deliver therapy to the heart.

25 Cardiac rhythm management systems include, among other things, pacemakers, also referred to as pacers. Pacers deliver timed sequences of low energy electrical stimuli, called pace pulses, to the heart, such as via an intravascular leadwire or catheter (referred to as a "lead") having one or more electrodes disposed in or about the heart. Heart contractions are initiated in response to such pace pulses

(this is referred to as “capturing” the heart). By properly timing the delivery of pace pulses, the heart can be induced to contract in proper rhythm, greatly improving its efficiency as a pump. Pacers are often used to treat patients with bradyarrhythmias, that is, hearts that beat too slowly, or irregularly. Such pacers may also coordinate atrial and ventricular contractions to improve pumping efficiency. Cardiac rhythm management systems also include cardiac resynchronization therapy (CRT) devices for coordinating the spatial nature of heart depolarizations for improving pumping efficiency. For example, a CRT device may deliver appropriately timed pace pulses to different locations of the same heart chamber to better coordinate the contraction of that heart chamber, or the CRT device may deliver appropriately timed pace pulses to different heart chambers to improve the manner in which these different heart chambers contract together.

Cardiac rhythm management systems also include defibrillators that are capable of delivering higher energy electrical stimuli to the heart. Such defibrillators include cardioverters, which synchronize the delivery of such stimuli to portions of sensed intrinsic heart activity signals. Defibrillators are often used to treat patients with tachyarrhythmias, that is, hearts that beat too quickly. Such too-fast heart rhythms also cause diminished blood circulation because the heart isn’t allowed sufficient time to fill with blood before contracting to expel the blood. Such pumping by the heart is inefficient. A defibrillator is capable of delivering a high energy electrical stimulus that is sometimes referred to as a defibrillation countershock, also referred to simply as a “shock.” The countershock interrupts the tachyarrhythmia, allowing the heart to reestablish a normal rhythm for the efficient pumping of blood. In addition to pacers, CRT devices, and defibrillators, cardiac rhythm management systems also include devices that combine these functions, as well as monitors, drug delivery devices, and any other implantable or external systems or devices for diagnosing or treating the heart.

One problem faced by cardiac rhythm management devices and other

implantable medical devices is in providing communication (i.e., telemetry) between the implanted device and a remote external interface device. The external interface device may be a dedicated or other programmer device used by a physician or other caregiver to interface with the implanted device. Such a bidirectional
5 communication link permits, among other things, programming of operational parameter(s) and/or executable code within the implanted device, and/or monitoring of device status indicator(s) and/or patient data. The present inventors have recognized that a long telemetry range is desired so that the physician or caregiver may, if desired, access the implanted device from a remote location. However,
10 using a far-field radio frequency (RF) communication link from an implanted medical device consumes significant power from the battery or other power source of the implanted medical device. This shortens the useful life of the implanted medical device before explantation and replacement becomes necessary. Moreover, a far-field RF signal transceived from an implanted location within the body faces
15 significant absorption of the transceived power by body tissue. This further increases the power required to obtain long range telemetry transception. For these and other reasons, the present inventors have recognized that there exists an unmet need for improved techniques of providing long-range telemetry using less power from the power source of the implanted device.

SUMMARY

This document discusses, among other things, a system, method, or device that includes an intermediary telemetry interface device for communicating between a cardiac rhythm management system or other implantable medical device and a
25 programmer or other remote device. One example provides an inductive near-field communication link between the telemetry interface and the implantable medical device, and a far-field radio-frequency (RF) far-field communication link between the telemetry interface device and the remote device. The telemetry interface device

provides data buffering. In another example, the telemetry interface device includes a data processing module, such as for compressing and/or decompressing data, or for extracting information from data. Such information extraction may include obtaining heart rate, interval, and/or depolarization morphology information from an electrogram signal received from the implantable medical device.

In one example, this document discusses an external telemetry interface device to assist in communication between an implantable medical device carrying an inductive element and an external remote first far-field radio-frequency (RF) transceiver. The telemetry interface device includes an inductive transceiver, configured to be communicatively coupled to the inductive element in the implantable medical device via a mutual inductance therebetween. It also includes a second far-field RF transceiver, configured to be communicatively coupled to the remote first far-field RF transceiver. It further includes a data buffer, coupled to the inductive and second far-field RF transceivers, to store data from the inductive and second far-field RF transceivers. Moreover, the telemetry interface device includes a controller, coupled to the inductive and second far-field RF transceivers and the data buffer, to issue control signals directing communication by the inductive and second far-field RF transceivers using data from the data buffer.

In another example, this document discusses an external telemetry interface device to assist in communication between an implantable medical device and a remote far-field radio-frequency (RF) transceiver. The telemetry interface device includes a first transceiver, configured to be communicatively coupled to the implantable medical device. It includes a second transceiver, configured to be communicatively coupled to the remote far-field RF transceiver. It also includes a data buffer, coupled to the first and second transceivers, to store data from the first and second transceivers. It further includes a controller, coupled to the first and second transceivers and the data buffer, to issue control signals directing communication by the first and second transceivers using data from the data buffer.

The controller includes a data processing module. The data processing module is configured to execute instructions to obtain extracted information, from electrogram data received from the implanted device via the first transceiver, for transmission by the second transceiver to the remote far-field RF transceiver.

5 This document also discusses a method of communicating between an implantable medical device and an external remote far-field RF transceiver. The method includes transceiving with the implantable medical device an inductively-coupled first communication signal. The method also includes transceiving with the external remote far-field RF receiver a second communication signal. The method
10 also includes buffering data received from at least one of the first and second communication signals.

 This document also discusses a method of communicating between an implantable medical device and an external remote far-field RF transceiver. The method includes transceiving with the implantable medical device a first
15 communication signal. It also includes extracting information from electrogram data included in the first communication signal. It further includes transceiving with the external remote far-field RF receiver a second communication signal. Other aspects of the invention will be apparent on reading the following detailed description of the invention and viewing the drawings that form a part thereof.

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BRIEF DESCRIPTION OF THE DRAWINGS

 In the drawings, which are offered by way of example, and not by way of limitation, and which are not necessarily drawn to scale, like numerals describe substantially similar components throughout the several views. Like numerals
25 having different letter suffixes represent different instances of substantially similar components.

 Figure 1 is a block diagram illustrating generally portions of a system including an implantable medical device, an external telemetry interface (I/F)

device, and a remote user interface device.

Figure 2 illustrates a technique of communication between an implantable medical device and a conventional medical device programmer using a near-field inductive communication link.

5 Figure 3 illustrates a technique of communication between an implantable medical device and a remote user interface via a telemetry interface device.

 Figure 4 illustrates a technique of communication: (1) between an implantable medical device and a telemetry interface device, using a near-field inductive communication link; (2) between a telemetry interface device and a
10 remote base station, using a far-field RF communication link; and (3) between a remote base station and a remote user interface, using a wired or wireless communication link.

 Figure 5 is a block diagram illustrating generally portions of an alternative system including an implantable medical device, an external telemetry interface (I/F)
15 device, and a remote user interface device.

 Figure 6 is a schematic/block diagram illustrating another example of a telemetry interface device that, in addition to transceiving a communication signal from an implantable medical device, also transceives a communication signal from another device, such as an external sensor, associated with or used by the patient.
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DETAILED DESCRIPTION

 In the following detailed description, reference is made to the accompanying drawings which form a part hereof, and in which is shown by way of illustration specific embodiments in which the invention may be practiced. These embodiments
25 are described in sufficient detail to enable those skilled in the art to practice the invention, and it is to be understood that the embodiments may be combined, or that other embodiments may be utilized and that structural, logical and electrical changes may be made without departing from the spirit and scope of the present invention.

The following detailed description is, therefore, not to be taken in a limiting sense, and the scope of the present invention is defined by the appended claims and their equivalents.

Figure 1 is a block diagram illustrating generally portions of a system 100 including an implantable medical device 105 (such as a cardiac rhythm management device), an external telemetry interface (I/F) device 110, and a remote user interface device 115 (such as a programmer and/or monitor for use with the implantable medical device 105) that includes a remote far-field radio-frequency (RF) transceiver 120. In this document, the terms “transceive,” “transceiving,” and “transceiver” refer to transmitting and/or receiving data. That is, these terms include all of: (1) transmitting, but not receiving; (2) receiving, but not transmitting; and, (3) both transmitting and receiving. Moreover, a “far-field,” which is also referred to as the Fraunhofer zone, refers to the zone in which a component of an electromagnetic field produced by the transmitting electromagnetic radiation source decays substantially proportionally to $1/r$, where r is the distance between an observation point and the radiation source. Accordingly, far-field refers to the zone outside the boundary of $r = \lambda/2\pi$, where λ is the wavelength of the transmitted electromagnetic energy. In one example, far-field RF telemetry is capable of communicating over a range that is at least six feet, but far-field RF communication may extend over a far greater distance.

In the example of Figure 1, telemetry IF device 110 includes an inductive transceiver 125, a random-access memory (RAM) or other data buffer 130, a far-field RF transceiver 135, a controller 140, and a power source 145 (such as a rechargeable or other battery). In this example, inductive transceiver 125 is wirelessly communicatively coupled by near-field link 150 to implantable medical device 105, using the mutual inductance coupling respective coils or other inductors. Far-field RF transceiver 135 is wirelessly communicatively coupled to remote user interface 115, using radiated far-field RF electromagnetic energy transmitted

between respective antennas by far-field communication link **155**. Because communication of data signals at links **150** and **155** may occur at different rates and/or may not be carried out concurrently, data buffer **130** performs data buffering in at least one direction, as directed by one or more control signals provided by controller **140**. Controller **140** is capable of sequencing through various control states such as, for example, by using a digital microprocessor having executable instructions stored in an associated instruction memory circuit, a microsequencer, or a state machine.

Telemetry interface device **110** may be worn or otherwise kept in close proximity to a patient in which implantable medical device **105** is implanted. In one example, telemetry interface device **110** is housed in an enclosure that fits in the patient's pocket or can be worn on a belt. Remote user interface **115** may be close to the patient (e.g., in the same room), or may be located at an extended distance from the patient. Far-field communication link **155** uses far-field RF energy, for example, at one or more ISM band frequencies (e.g., about 902 MHz to 928 MHz), ISM/BLE frequencies (e.g., about 2.4 GHz to 2.5 GHz), cell phone band frequencies (e.g., Advanced Mobile Phone System (AMPS) at about 824 MHz to 894 MHz, Personal Communication Services (PCS) at about 1.8 GHz to 2.0 GHz, etc.), two-way pager band frequencies (e.g., 930 MHz to 950 MHz), and/or Global System for Mobile (GSM) frequencies at about 1.85 GHz to 1.99 GHz. Far-field communication link **155** uses a mutual inductance coupling implantable device **105** to telemetry interface device **110**. This configuration of system **100** advantageously permits implantable device **105** to also communicate, using a mutual inductance, to an existing inductively-coupled implantable medical device programmer, as well as to telemetry interface device **110**.

Figure 2 illustrates a technique of communication between implantable medical device **105** and a conventional medical device programmer **200** (before device **105** is implanted in a patient), using near-field inductive communication link

150. For example, such communication may be used to program parameters of implantable medical device **105** using a user-interface of programmer **200**. In another example, such communication may be used to obtain device status information at programmer **200** from implantable medical device **105**.

5 Figure 3 illustrates a technique of far-field RF communication between implantable medical device **105** and remote user interface **115** (such as, for example, a medical device programmer **200** having both far-field RF and inductive transceiver capabilities), via telemetry interface device **110**. Implantable medical device **105** and telemetry interface device **110** are communicatively linked by near-field inductive communication link **150**. Telemetry interface device **110** and remote user interface **115** are communicatively linked by far-field RF communication link **155**. In one example, such communication occurs during or immediately after the implantation of implantable medical device **105** into a patient, or during a subsequent follow-up visit by the patient to the doctor or other care-giver.

15 Figure 4 illustrates a technique of communication: (1) between implantable medical device **105** and telemetry interface device **110**, using a near-field inductive communication link **150**; (2) between telemetry interface device **110** and remote base station **400**, using a far-field RF communication link **155**; and (3) between remote base station **400** and a remote user interface (or data management server) **405**, using a wired communication link **410** (e.g., telephone lines, internet connection, etc.) or a wireless communication link (e.g., cell phone link, far-field RF link, etc.). In this example, remote base station **400** includes a remote far-field RF transceiver **120** and a network interface **415** coupled thereto. Network interface **415** includes a modem or other suitable device that is adapted for communication over
20 the wired or wireless communication link **410**. Remote user interface **405** may include a medical device programmer **200**, operated by a doctor or other care-giver. Alternatively, remote user interface **405** may include a data management server for storing physiological data, device status data, or other data received from
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implantable medical device **105**, or for automatically providing programmable parameters to configure implantable medical device **105**.

Figure **5** is a block diagram illustrating generally portions of an alternative system **500** including an implantable medical device **505**, an external telemetry interface (I/F) device **510**, and a remote user interface device **115** (such as a programmer and/or monitor for use with the implantable medical device **505**) that includes a remote far-field radio-frequency (RF) transceiver **120**. In the example of Figure **5**, telemetry IF device **510** includes a far-field RF or an inductive transceiver **525**, a random-access memory (RAM) or other data buffer **130**, a far-field RF transceiver **135**, a controller **540**, and a power source **145**. In this example, transceiver **525** is wirelessly communicatively coupled by far-field RF or near-field inductive communication link **550** to implantable medical device **505**. Far-field RF transceiver **135** is wirelessly communicatively coupled to remote user interface **115**, using radiated far-field RF electromagnetic energy transmitted between respective antennas by far-field link **155**. Because data communication at links **550** and **155** may occur at different rates and/or may not be carried out concurrently, data buffer **130** performs data buffering in at least one direction, as directed by one or more control signals provided by controller **540**.

Controller **540** includes a data processing module **590**. In one example, data processing module **590** performs executable steps for compressing and/or decompressing data being buffered in data buffer **130** for communication to and/or from implantable medical device **505**. In one such example, telemetry interface device **510** receives physiological data (e.g., an cardiac signal electrogram) over an extended period of time, and data processing module **590** uses Huffman encoding or another suitable data compression technique to compress the data before communicating it to remote user interface **115**.

In another example, communication at link **550** operates using a high efficiency communication protocol tailored for communication with implantable

device 505. In this example, data processing module 590 translates the data from implantable device 505, as needed, to enable far-field RF communication at far-field communication link 155 using a standardized communication protocol. In this example, such processing by data processing module 590 may include stripping a header on data received from implantable device 505 over link 550, and adding a TCP/IP or other standardized header to data being communicated over far-field RF communication link 155 to remote user interface 115.

In one example, device 505 occasionally or periodically transmits, to telemetry interface device 510, physiological information, such as electrogram information about one or more cardiac signals sensed at one or more patient electrodes. Data processing module 590 includes a level-detection or other suitable algorithm for detecting cardiac depolarizations included in the cardiac signal. Using this extracted information about heart depolarizations, data processing module 590 calculates average heart rate, the values of the time intervals between successive heart depolarizations, and/or morphology information about the depolarizations. Other processing by data processing module 590 may include, among other things: calculating heart rate variability (e.g., for diagnosing patient wellness), recognizing and/or classifying an arrhythmia (e.g., atrial flutter, atrial fibrillation, etc.) or other characteristic of the cardiac signal (e.g., QT alternans, etc.). Such processing may also include a comparison of a characteristic to a threshold value, or any other suitable technique for generating an alert condition that is communicated to a physician or other caregiver at remote user interface 115, using far-field RF communication link 155.

Such information extracted from the heart depolarizations is then transmitted by far-field RF transceiver 135 to remote user interface 115 via far-field RF communication link 155, as an alternative to transmitting all of the source electrogram data. Examples of extracting depolarization morphology information are found in Hsu et al. U.S. Patent No. 6,275,732 entitled MULTIPLE STAGE

MORPHOLOGY BASED SYSTEM DETECTING VENTRICULAR
TACHYCARDIA AND SUPRAVENTRICULAR TACHYCARDIA and Hsu et al.
U.S. Patent No. 6,266,554 entitled SYSTEM AND METHOD FOR CLASSIFYING
CARDIAC COMPLEXES, each of which is assigned to Cardiac Pacemakers, Inc.,
5 and each of which is incorporated by reference herein in its entirety, including its
description of using cardiac features and/or morphology information.

In another example in which device **505** regularly transmits to telemetry
interface device **510** physiological information (e.g., electrogram information about
one or more cardiac signals sensed at one or more patient electrodes, and/or
10 information from one or more physiological sensors such as an accelerometer, a
minute ventilation sensor, etc.), telemetry interface device **510** processes the
physiological data to compute one or more indicators of patient wellness, which are
then transmitted by far-field RF transceiver **135** to remote user interface **115** via far-
field RF communication link **155**. One example of processing physiological and/or
15 sensor data to determine an indicator of patient wellness is described in Carlson et
al. U.S. Patent Application Serial No. 09/802,316, entitled CARDIAC RHYTHM
MANAGEMENT SYSTEM USING TIME DOMAIN HEART RATE
VARIABILITY INDICIA, filed on March 8, 2001, which is incorporated by
reference herein in its entirety, including its description of determining indications
20 of patient wellness. In one example, telemetry interface device **510** is used to
communicate an alert to a doctor or other caregiver using remote user interface **115**
when the patient becomes unwell, such as when a patient wellness indicator crosses
a predetermined threshold value. In one example, a QT interval length obtainable
from a cardiac signal is used as a patient wellness indicator, and telemetry interface
25 device **510** alerts a physician at remote user interface **115** when the QT interval
length exceeds a predetermined threshold value or exhibits QT alternans (i.e., a
pattern of successive alternating long-short QT intervals).

In yet another example in which device **505** regularly transmits to telemetry

interface device **510** physiological information (e.g., electrogram information about one or more cardiac signals sensed at one or more patient electrodes, and/or information from one or more physiological sensors such as an accelerometer, a minute ventilation sensor, etc.), telemetry interface device **510** processes the physiological data to predict whether a future arrhythmia is likely to occur. This information is then either transmitted from telemetry interface device **510** to remote user interface **115** via far-field RF communication link **155**, such as to notify a physician or other caregiver, and/or is transmitted back to implanted device **505** to trigger therapy that prevents the arrhythmia from occurring. One example of processing physiological and/or sensor data to predict and/or prevent an arrhythmia is described in Sweeney et al. U.S. Patent No.6,272,377, entitled CARDIAC RHYTHM MANAGEMENT SYSTEM WITH ARRHYTHMIA PREDICTION AND PREVENTION, which is incorporated by reference herein in its entirety, including its description of providing arrhythmia prediction and prevention techniques.

Figure **6** is a schematic/block diagram illustrating another example of a telemetry interface device **510** that, in addition to transceiving a communication signal from an implantable device **505**, also transceives a communication signal with another device **610** (such as an external sensor) associated with or used by the patient. In this example, telemetry interface device **510** includes a transceiver **600** for transceiving a communication signal, at **605**, from another device **610** associated with or used by the patient. In one example, device **610** is a scale including a far-field RF transceiver communicating, at **610**, information about the patient's weight to far-field RF transceiver **600** in telemetry interface device **510**. Telemetry interface device communicates this information and information from implantable device **505** to remote far-field RF transceiver **120**. Other examples of device **610** include an external pressure sensor (e.g., a cuff on the patient's finger), an external respiration monitor, or any other sensor providing information about the patient. By

communicating information from both implantable device **505** and external device **610** to remote user interface **115**, telemetry interface device **510** enhances the information available to the physician or other caregiver using remote user interface **115**. Telemetry interface device **510** may further perform processing, using data processing module **590**, of data from both implantable device **505** and external device **610** that includes correlating data from both of these sources. This also further enhances the information available to the physician or other caregiver using remote user interface **115**. In one example, transceiver **600** is shared or combined with one of transceivers **525** or **135**.

It is to be understood that the above description is intended to be illustrative, and not restrictive. For example, the above-discussed embodiments may be used in combination with each other. Many other embodiments will be apparent to those of skill in the art upon reviewing the above description. The scope of the invention should, therefore, be determined with reference to the appended claims, along with the full scope of equivalents to which such claims are entitled. In the appended claims, the terms “including” and “in which” are used as the plain-English equivalents of the respective terms “comprising” and “wherein.” Moreover, the terms “first,” “second,” “third,” etc. are used merely as labels, and are not intended to impose numeric requirements on their objects.